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An automated pipeline for bouton, spine, and synapse detection of in vivo two-photon images

Qiwei Xie^{1,2,3†}, Xi Chen^{3†}, Hao Deng⁴, Danqian Liu⁵, Yingyu Sun⁶, Xiaojuan Zhou⁶, Yang Yang^{5,7*} and Hua Han^{3,7,8*}

*Correspondence:

yangyang@ion.ac.cn;
hua.han.casia@gmail.com

†Equal contributors

⁵Institute of Neuroscience, Chinese Academy of Sciences, 320 Yue Yang Road, 200031 Shanghai, China

³Institute of Automation, Chinese Academy of Sciences, 95 Zhongguancun East Road, 100190 Beijing, China

Full list of author information is available at the end of the article

Abstract

Background: In the nervous system, the neurons communicate through synapses. The size, morphology, and connectivity of these synapses are significant in determining the functional properties of the neural network. Therefore, they have always been a major focus of neuroscience research. Two-photon laser scanning microscopy allows the visualization of synaptic structures in vivo, leading to many important findings. However, the identification and quantification of structural imaging data currently rely heavily on manual annotation, a method that is both time-consuming and prone to bias.

Results: We present an automated approach for the identification of synaptic structures in two-photon images. Axon boutons and dendritic spines are structurally distinct. They can be detected automatically using this image processing method. Then, synapses can be identified by integrating information from adjacent axon boutons and dendritic spines. In this study, we first detected the axonal boutons and dendritic spines respectively, and then identified synapses based on these results. Experimental results were validated manually, and the effectiveness of our proposed method was demonstrated.

Conclusions: This approach will be helpful for neuroscientists to automatically analyze and quantify the formation, elimination and destabilization of the axonal boutons, dendritic spines and synapses.

Keywords: in vivo two-photon imaging, Synapse, Bouton, Spine, Image enhancement

Introduction

Synapses were first discovered in the 1890s, when Sir Sherrington, through his pioneering work on motor reflexes, wrote that synapse is the way of neuronal communication in the nervous system [1]. There are two major types of synapses: chemical and electrical. In the mammalian central nervous system, the vast majority of the synapses are chemical. Chemical synapses, especially excitatory synapses, typically consist of presynaptic axon boutons and postsynaptic dendritic spines. The structural plasticity of boutons and spines underlies functional synaptic plasticity, widely accepted as the neural basis of learning and memory. Brain imaging can be used to characterize changes occurring in a brain during very different time-scales [2]. The advent of boutons and spines can be imaged in

live animals over days or even months, allowing observation of structural changes *in vivo*, often in direct association with learning [3–11].

Manual validation is extremely time-consuming, and error prone. Meanwhile, different criteria may lead to different results. Therefore, manual methods are not suitable for the processing of large-scale data. The recent advances in biomedical imaging have allowed the initial development of computer-aided semiautomatic or automatic approaches to detect dendritic spines based on image analysis. In [12], Xie et al. proposed an algorithm for automatic neuron reconstruction. The algorithm can handle complex structures adaptively and optimize the localization of bifurcations. In [13], an automated scheme to perform segmentation in a variational framework was proposed to trace neurons from confocal microscopy images. The segmentation framework, referred to as “tubularity flow field (TuFF)”, performs directional regional growing guided by the direction of tubularity of the neurites. In [14], a robust automatic neuron segmentation and morphology generation algorithm was proposed. The algorithm-Tree2Tree uses a local medial tree generation strategy in combination with a global tree linking to build a maximum likelihood global tree. It is a reliable technique to compare various of neurons for tracing evaluation and neuron retrieval. Gonzalez et al. presented an approach to fully automated delineation of tree structures in noisy 2D images and 3D image stacks. It is able to eliminate noise while retaining the right tree structure [15]. Besides, in [16], Gonzalez et al. showed that using steerable filters to create rotationally invariant features that include higher-order derivatives, and training a classifier based on these features allows us handle such irregular structures. Rodriguez et al. developed an open-source software NeuronStudio to aid the neuroscientist in the task of reconstruction of neuronal structures from confocal and multi-photon images [17]. It is a self-contained software package that is free, easy to use. The focus of previous work mentioned above varies, with some focusing on neuronal tracking, segmentation and others on specific situations.

They inspired us to explore 3D tracking, segmentation and extraction of synapses both in 2D and 3D based on the detection results of our automatic detection method. Therefore, it is of interest to explore methods of automatic detection and quantification of synapses, dendrites and axons.

In addition to examining boutons and spines separately by two-photon microscopy, it is also possible to visualize synaptic connections with identified boutons and spines that are in close proximity. Although the resolution of light microscopy is larger than the size of the synaptic cleft, previous studies have showed that over 85% of putative synapses identified in deconvoluted confocal images were true synapses confirmed using electron microscopy [18]. Light microscopy can still provide useful information. Given that boutons and spines originated from different brain regions or of different cell types can be labeled using different fluorescent proteins, observation of synaptic connections using two-photon microscopy provides a valuable method for researching long-range and cell-type specific synaptic plasticity *in vivo* [19]. Therefore the automated detection of synapses will be of tremendous help for this kind of data analysis.

In this paper, we focus on the detection of axonal boutons, dendritic spines and synapses from the *in vivo* two-photon image stacks. As described above, a synapse typically consists of one axonal bouton and one dendrite spine, with the exception of multi-bouton and multi-spine synapses. A reasonable strategy to locate the synapses is to first detect axonal boutons and dendritic spines, then to search for synaptic contacts composed of

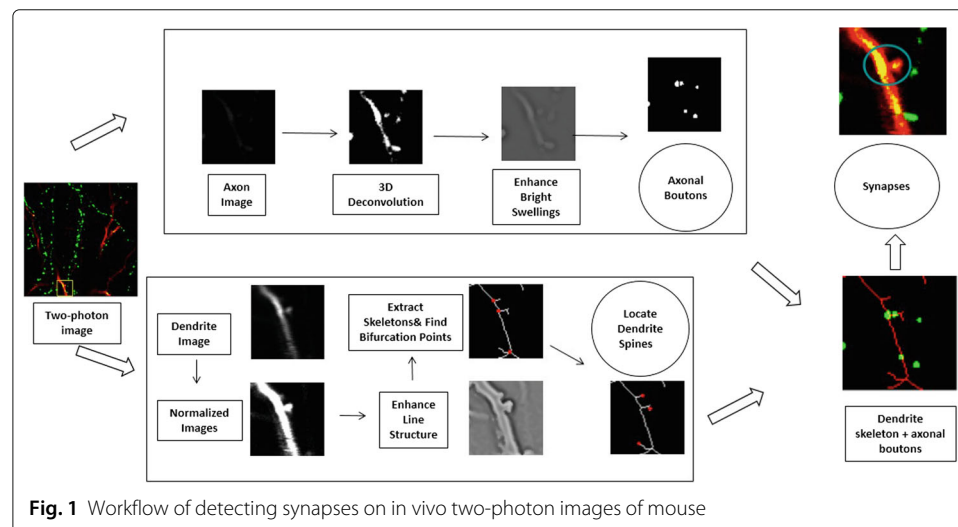
bouton and spine pairs. A robust Gaussian model was used in order to enhance the morphology of axonal boutons and dendrites respectively, while effectively inhibiting noise. Before the enhancement operation, we performed deconvolution on axon images as a pre-processing method for noise reduction. And the regions with relatively higher values are regarded as axonal boutons with great possibility. For the detection of dendritic spines, we performed one-threshold segmentation to obtain the structure of the dendrites based on the enhanced images of dendrites, which followed by an efficient thinning algorithm. After we extracted the centerline of the dendrites, the dendritic spines were determined by finding the bifurcation points and endpoints.

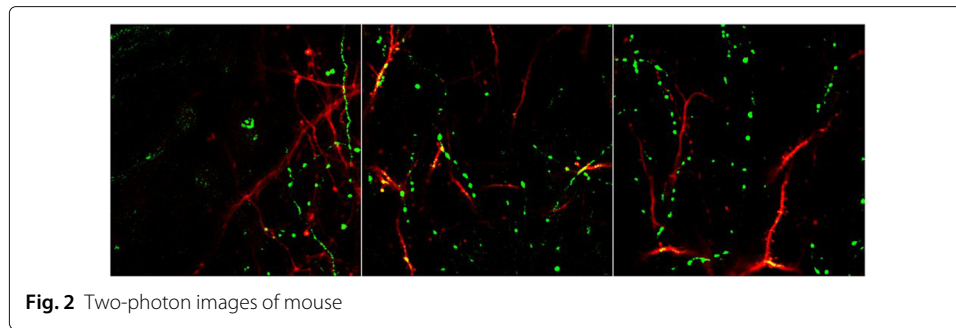
Material and method

Figure 1 illustrates the workflow of our proposed approach for detection of synapses. We will give a detailed description of each procedure of the method after the introduction to the image stack in this paper.

Materials

The image data used in this study was obtained from Institute of Neuroscience, State key Laboratory of Neuroscience, Chinese Academy of Sciences, Center for Excellence in Brain Science and Intelligence Technology. The transgenic mice (YFP-H line), both male and female, were imaged using a two-photon microscope (Sutter), controlled by Scanimage (Janelia). Auditory cortex of mice was exposed surgically and covered with glass cranial window for repeated two-photon imaging in vivo. Surgical details refer to Y. Yang [19]. Image stack was acquired from the cortical surface to 100–150 μm depth with 0.7 μm intervals. A 25 \times objective with 1.05 numerical aperture was used (Olympus). A Ti:sapphire laser (Spectra-Physics) was used as the light source, and tuned to 92 nm for imaging. YFP (Yellow Fluorescent Protein) and GFP (Green Fluorescent Protein) signals were collected using filters 495/40 and 535/50 (Chrome). The 535/50 filter (Channel 1) collected both GFP and YFP signals, and the 495/40 filter (Channel 2) collected GFP-only signals. By subtracting the GFP signals from Channel 1 signals, the YFP-only images were obtained [19].





The dual-color images, as shown in Fig. 2, are the two-photon images, where the red section and green section represent YFP (containing dendrites and axons) and GFP images (contains long-range projecting axons only) respectively and the spine-bouton pairs are thought to be synapse. The x - y resolution and the z resolution of the image data are 137 nm/pixel and 700 nm/pixel respectively, and the image size (x - y) is 512-by-512.

Detection of axonal boutons

In this section, we provide algorithmic details for axonal bouton detection. The proposed algorithm is divided into three parts. First, a 3D deconvolution operation is required due to the noise in the original image stacks. Next, we enhanced the bright swellings in the deconvolved images and segmented them. Finally, we identified true axonal boutons based on a series of criteria. The whole workflow for detecting axonal boutons is shown in Fig. 3.

Algorithm 1 Detection of axonal boutons

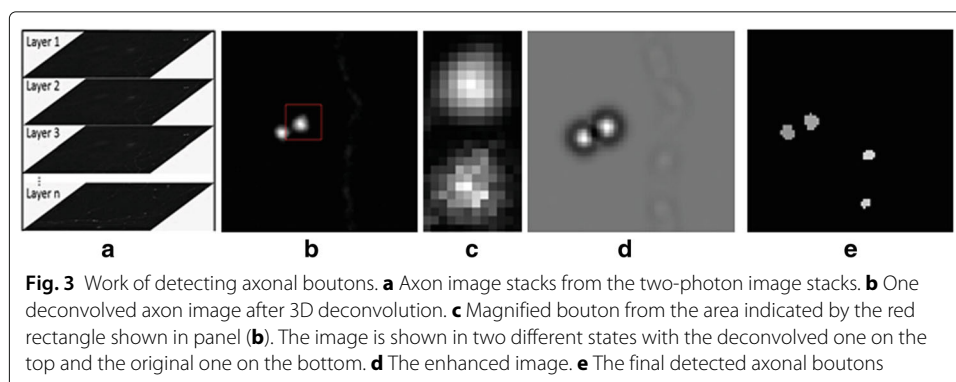
Input: In vivo two-photon images of axons $\{\phi\}$.

for each image $\in \{\phi\}$ **do**

- 1 Deconvolution by the steps described in the [Appendix 3D deconvolution];
- 2 Enhance the bright swellings with Algorithm 2;
- 3 Locate the axonal boutons with Algorithm 3;

end for

Output: Set of coordinates of the points of axonal boutons Δ .



3D deconvolution

Although confocal microscopy images are known to be sharper than standard epifluorescence ones, they are still inevitably degraded by Poisson noise and residual out-of-focus light due to photon-limited detection [20]. Thus, several deconvolution methods have been proposed. In this study, we adopt the Deconvolution Approach for the Mapping of Acoustic Sources (DAMAS), which decouples the array design and processing influence from the noise being measured using a simple and robust algorithm [21]. The details of 3D deconvolution operation implemented in ImageJ [22] are shown in Appendix.

One deconvolved axon image is depicted in Fig. 3b. To demonstrate the performance of the 3D deconvolution operation, we show an axonal bouton indicated by the red rectangle in Fig. 3b. We then show two different states of this image in Fig. 3c, with the deconvolved one on the top and the original one on the bottom. A significant difference can be seen from the detailed comparison, showing that the 3D deconvolution operation helps to identify the axonal boutons.

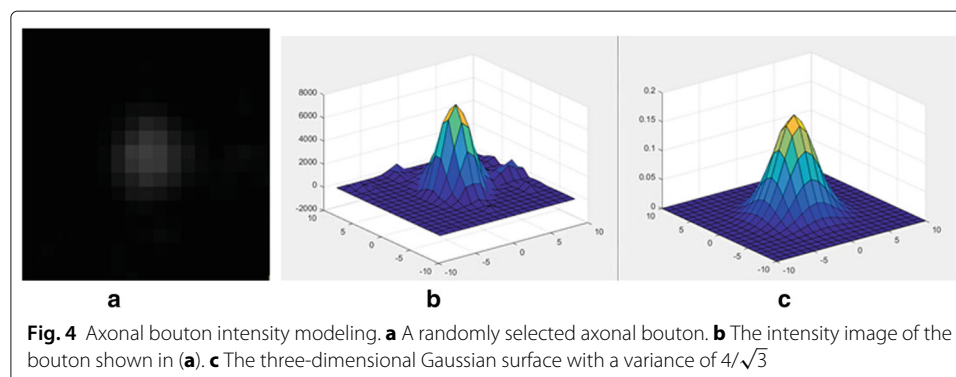
Enhancing bright swellings

The thresholding on a deconvolved image does not necessarily ensure perfect segmentations, or even good ones. This is because the range of the intensity of different axonal boutons can vary dramatically. A low threshold will reserve the bright axon shaft, but a high threshold will eliminate weak axonal boutons. To avoid the loss of data, we first enhanced the bright swellings.

By the statistics carried on the corresponding electron microscope data, the average diameter of terminal boutons is $1.0 \mu\text{m}$. By setting the pixel size to 137 nm, we find the average radius of an axonal bouton is about 4 pixels. We randomly select an axonal bouton as shown in Fig. 4a and show the plot of its corresponding intensity image in Fig. 4b. Note that the axonal bouton is a “rounded” profile. We can see that the image in Fig. 4b looks very similar to the three-dimensional Gaussian surface plotted in Fig. 4c, suggesting it is reasonable to model the intensity of axonal bouton using a three-dimensional Gaussian surface,

$$R(x, y) = C \exp\left(-\frac{(x - x_0)^2 + (y - y_0)^2}{2\delta^2}\right), \quad (1)$$

where C is a constant corresponding to the coordinate of the maximum magnitude point (x_0, y_0) , and δ is the variance of the Gaussian surface. A very small part of the axonal boutons can be approximated by a ridge, we then construct a Hessian-based ridge detector.



Let $m = (x - x_0)^2 + (y - y_0)^2$. The intensity of enhanced image is set as additive inverse of the eigenvalue with minimum absolute, i.e. [Appendix A],

$$\lambda(m) = \begin{cases} -\exp\left(-\frac{m}{2\delta^2}\right) \left(m - 2\delta^2 + \sqrt{(m + 2\delta^2)^2 - 4\delta^4}\right) / 2\delta^5, & m \leq 2\delta^2 \\ -\exp\left(-\frac{m}{2\delta^2}\right) \left(m - 2\delta^2 - \sqrt{(m + 2\delta^2)^2 - 4\delta^4}\right) / 2\delta^5, & m > 2\delta^2. \end{cases} \quad (2)$$

Here we analyze in three cases:

- 1) : $m = 0, \lambda(m) = 1/\delta^3$;
- 2) : $m = 2\delta^2, \lambda(m) = -\sqrt{3}/(\delta^3 \times e)$, where e is the Euler's number;
- 3) : $m \rightarrow \infty, \lambda(m) = 0$.

For the parabolic line profile, the magnitude of the second derivative of the extracted position is always maximum at the line position [23]. We can conclude that the relationship between the variance δ and the radius r of the axonal bouton is $\delta = r/\sqrt{3}$ [Appendix B]. Combined with the radius of axonal boutons, we set the variance as $\delta = r/\sqrt{3}$ in this study.

To allow visual interpretation, we plot the chosen eigenvalue of model (1) in Fig. 5, from which we can see that the central region is enhanced while the surrounding region weakens gradually. This provides the theoretical basis for image enhancement and segmentation. Inspired by [23–25], we select the above variance. Figure 3 depicts the enhanced image of one bright swelling, whose variation tendency consistently conforms to that of Fig. 3 almost everywhere, supporting the correctness of our theoretical analysis. Compared to the image in Fig. 3b, the enhanced image shown in Fig. 3d has an advantage for weaker axonal boutons because of its more obvious profile. The following work is based on the enhanced image in Fig. 6, and the detail is stated in Algorithm 2.

Algorithm 2 Enhancing bright swellings

Input: Deconvolved image ϕ_{dec} .

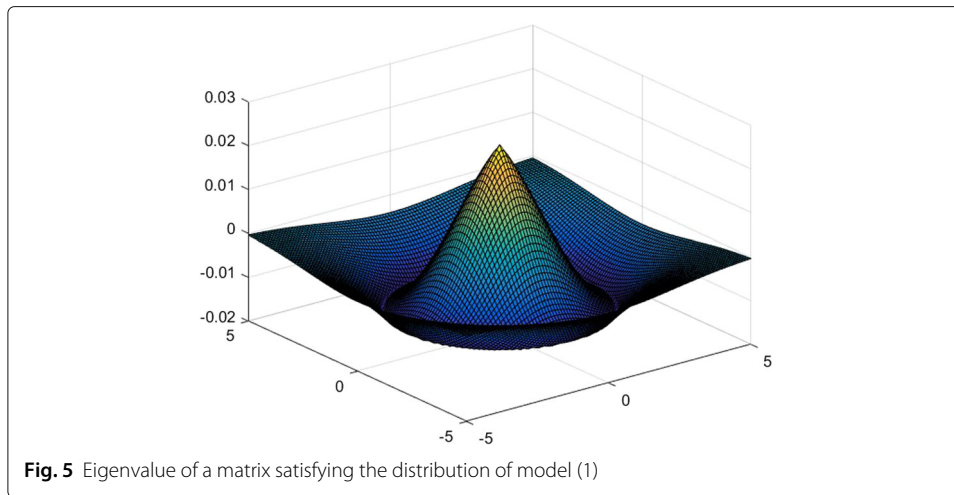
- 1 Compute the second partial derivatives $R_{xx}, R_{xy}, R_{yx}, R_{yy}$ with Eq. (6);
- 2 Calculate the eigenvalues λ_a of Hessian matrix with Eq. (7);
- 3 Choose the value to be the pixel value of the enhanced image with Eq. (2);

Output: Enhanced image ϕ_{enh} .

Obtaining axonal boutons

As discussed in last section, the application of a relatively lower threshold will inevitably generate false positives. Fortunately, the shapes of the axonal boutons are homogeneous and each has a sole maximum point. Therefore, we first find local maximum points as candidate points for axonal boutons, a simple but effective strategy. The detail is stated in Algorithm 1.

We then evaluate whether each region in the resulting segmentation contains a local maximum points and we delete the regions lacking local maximum points. On this basis, we compute some statistical characteristics including the eccentricity, major axis, and minor axis. Then we reserve the regions that exhibit statistical characteristics similar to a disk. Finally, we record the location of the reserved regions and determine whether the

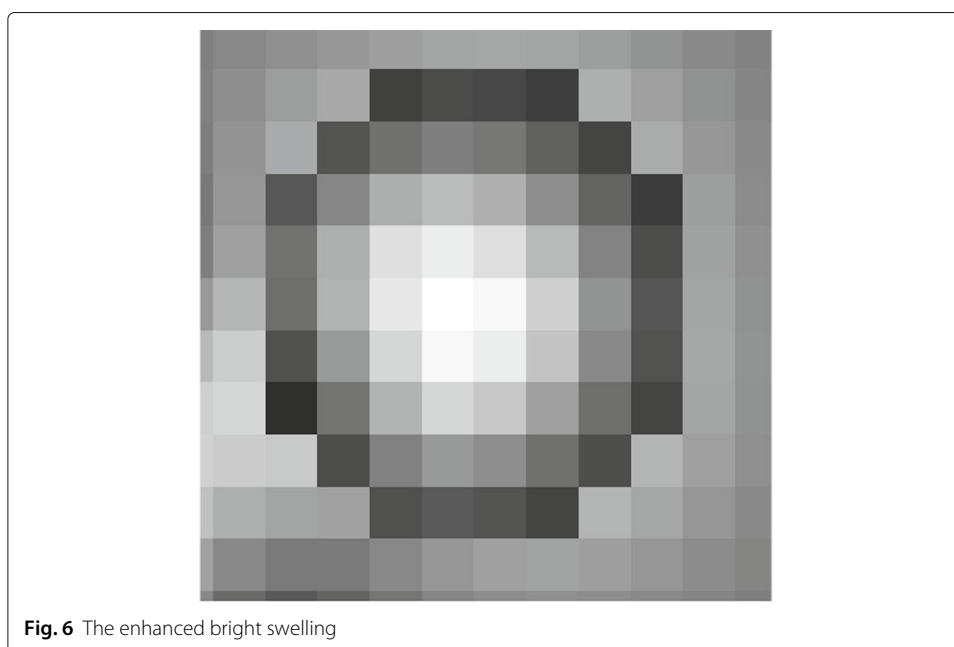


peak intensity of each region is more than three times brighter than its axon shaft in the original image [19]. The final result of axonal boutons analysis is shown in Fig. 3e.

Detection of dendritic spines

In this section, we explicate the details of our method for the detection of dendritic spines. Dendritic spines are small with spine head volumes ranging from $0.01 \mu\text{m}^3$ to $0.8 \mu\text{m}^3$. According to the shape, dendritic spines can be classified into following types: thin, mushroom, and stubby, as shown in Fig. 7 [26]. The variable shape of these spines is related to the strength and maturity of the synapses [27]. Thus, based on the forms, it is reasonable to locate the dendritic spines by looking for the spur pixels that are connected to the bifurcation points.

The proposed algorithm consists of three parts: enhancement of the line structure in the images after pretreatment; segmentation of dendrites and extraction of their skeletons;



Algorithm 3 Locating axonal boutons

Input: Original image ϕ , deconvolved image ϕ_{dec} and corresponding enhanced image ϕ_{enh} .

Initialize $\Delta' = []$, $\Delta = []$.

- 1 Binaryzation: $B_a = \phi_{dec} > T_a$;
- 2 Add the brightest points $\{pm\}$ in connected regions of B_a to Δ' ;
- 3 Determine the axonal boutons;
 - **for** each point $pm \in \Delta'$ **do**
 - Focus on the connected region that contains pm in ϕ_{delta} , represented as D_{pm} , and the corresponding region in ϕ , represented as ϕ_{pm} ;
 - if** the D_{pm} is disk-like
 - & the peak intensity in ϕ_{pm} is over three times brighter than its axon shaft **then**
 - Add pm into Δ ;
 - end if**
 - **end for**

Output: Set of coordinates of candidate points in axonal boutons Δ .

and identification of the dendritic spines based on the dendritic skeletons. The workflow is shown in Fig. 8 and Algorithm 4.

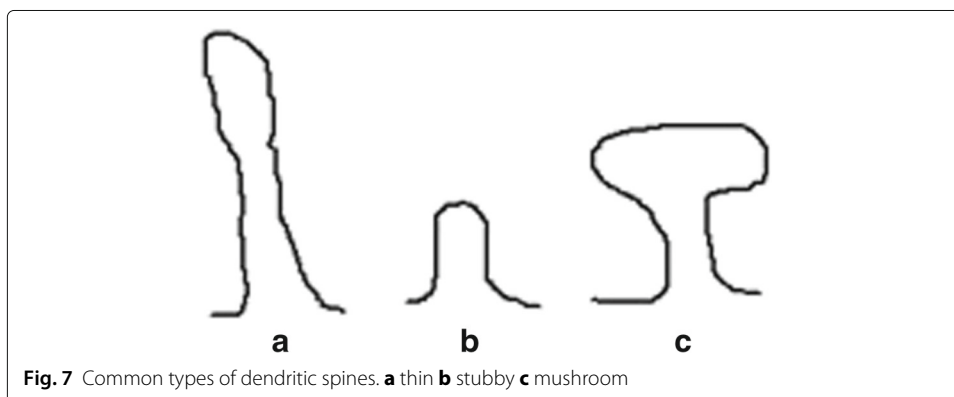
Enhancing line structure

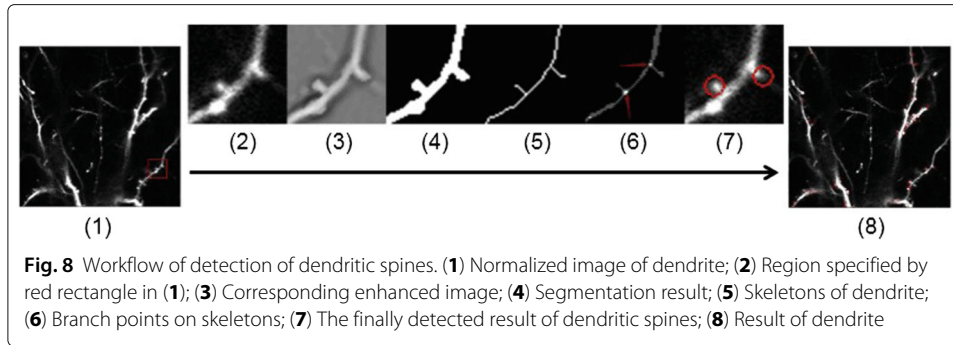
Before performing other operations, we first normalize the images to reduce the impact of noise by using the following formula:

$$I(x, y) = \frac{I(x, y) - I_{min}}{I_{max} - I_{min}}, \quad (3)$$

where $I(x, y)$ is the intensity value in I at (x, y) , I_{max} and I_{min} represent the maximum intensity and minimum intensity value of the image respectively.

Next, we enhance the linear structure. As shown in Fig. 9, the intensity value of each section of the dendritic linear structure can be modeled as a Gaussian curve [23], which can be written as





Algorithm 4 Detection of dendritic spines

Input: In vivo two-photon images of dendrite $\{Img\}$.

Initialize $\Omega' = []$, $\Omega = []$.

for each image I in $\{Img\}$ **do**

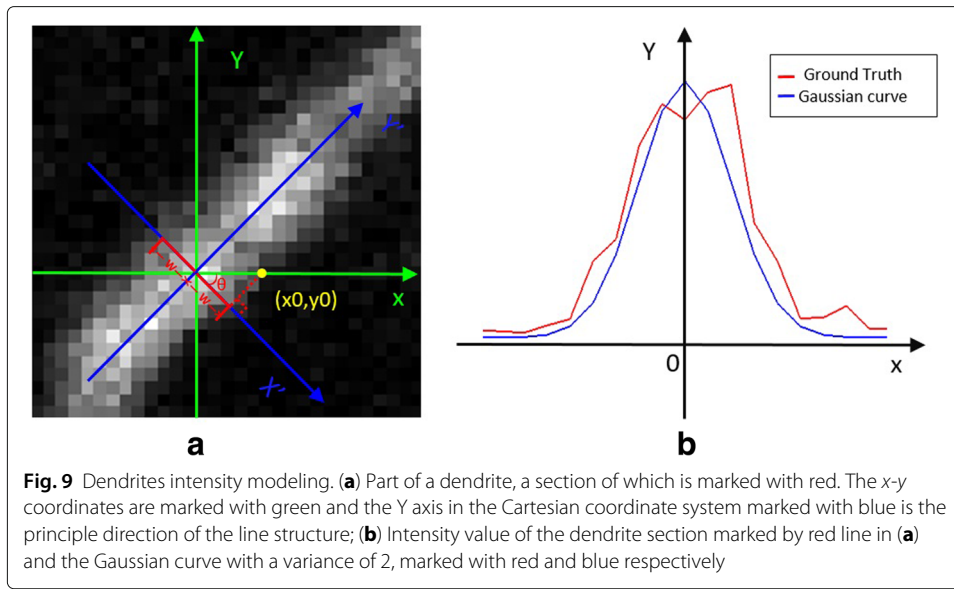
- 1 Normalize I using Eq. (3);
- 2 Enhance linear structures with Algorithm 5;
- 3 Extract skeletons of linear structures with Algorithm 6;
- 4 Look for branch points on the skeletons:
 - Compute convolution of the skeleton figure and a 3-by-3 filter, and denote by C the result;
 - Take the points whose intensity value is equal or greater than 4 on C as branch points, represent as $Pb = \{pb\}$;
- 5 Find dendritic spines on the skeletons:
 - Represent spur pixels on C as $Ps = \{ps\}$;
 - **for** each $ps \in Ps$ **do**
 - Focus on the regions on C that centered on ps ;
 - if** $ps \in Ps$ and arbitrary $pb \in Pb$ are connected by skeleton **then**
 - Add ps to Ω' ;
 - end if**
 - **end for**
- 6 Filtrate false positives on axons with Algorithm 7;

end for

Output: Set of coordinates of dendritic spines Ω .

$$I(x') = C_{den} \exp\left(-\frac{x'^2}{2\sigma^2}\right) = C_{den} \exp\left(-\frac{(x \cos \theta - y \sin \theta)^2}{2\sigma^2}\right), \quad (4)$$

where x' is the abscissa on Cartesian coordinate system $X'-Y'$; x, y are the abscissa and ordinate on Cartesian coordinate system $X-Y$, respectively; C_{den} is the maximum pixel value of the cross section; σ is the variance of the Gaussian curve, and θ is the angle between the cross section and the main direction of the linear structure, which is shown in Fig. 9a. According to [23], we can obtain the relationship between the variance σ and the radius of the lines structure w [Appendix C]: $\sigma = w/\sqrt{3}$.



The average diameter of the dendritic spine of the part is less than $0.9 \mu\text{m}$, while the x - y resolution is 137 nm/pixel , so the average radius w is equal to 3 pixels.

As in previous part, we construct a Hessian-based ridge detector and take the additive inverse of the eigenvalue with maximum absolute value as the intensity of the enhanced image [Appendix D]:

$$I_{enh}(x, y) = \begin{cases} -\sigma^2 \lambda(x, y), & \text{if } \lambda(x, y) < 0 \\ 0, & \text{otherwise} \end{cases} \quad (5)$$

The approach for enhancing line structure can be summarized as follows:

Algorithm 5 Enhancing Linear structures

Input: A normalized in vivo two-photon image of dendrite I , output from step 1 in Algorithm 4.

- 1 Model the intensity values of I with Eq. (4);
- 2 Compute the Hessian matrix H with Eqs. (12, 13), and obtain the eigenvalues λ_d ;
- 3 Obtain pixel value of enhanced image with Eq. (5);

Output: Enhanced in vivo two-photon image of dendrite I_{enh} .

Extracting skeleton and finding branch points

We use the following Algorithm 6 to get the dendritic skeleton C (Fig. 8(5)) at the basis of the binary image B (Fig. 8(4)), which is obtained by segmenting the enhanced image I (Fig. 8(3)) using a suitable threshold [28]:

1. In the first sub-iteration, delete pixel p if and only if the condition (a), (b), (c) are all satisfied.
2. In the second sub-iteration, delete pixel p if and only if the condition (a), (b), (d) are all satisfied.

- Condition (a): $X_H(p) = 1$
 where $X_H(p) = \sum_{i=1}^4 b_i$, $b_i = \begin{cases} 1, & \text{if } x_{2i-1} = 0 \text{ and } (x_{2i} = 1 \text{ or } x_{2i+1} = 1) \\ 0, & \text{otherwise} \end{cases}$
 x_1, x_2, \dots, x_8 are the values of the eight neighbors of p , starting from the east neighbor and numbered in counter-clockwise order.
- Condition (b): $2 \leq \min\{n_1(p), n_2(p)\} \leq 3$,
 where $n_1(p) = \sum_{k=1}^4 x_{2k-1} \cup x_{2k}$, $n_2(p) = \sum_{k=1}^4 x_{2k} \cup x_{2k+1}$.
- Condition (c): $(x_2 \cup x_3 \cup \bar{x}_8) \cap x_1 = 0$
- Condition (d): $(x_6 \cup x_7 \cup \bar{x}_4) \cap x_5 = 0$

The two sub-iterations together make up one iteration of the algorithm and the iterations are repeated until the resulting image stops changing. The approach for extracting skeletons can be summarized as follows:

Algorithm 6 Extracting dendritic skeleton

Input: Enhanced in vivo two-photon image of dendrite I_{enh} .

- 1 Binaryzation: $B = I_{enh} > t$;
- 2 Eliminate redundant points:
 - **for** each pixel $p \in B$ **do**
 - if** condition (a) (b) (c) are satisfied **then**
 - delete p ;
 - end if**
 - **end for**
 - **for** each pixel $p \in B$ **do**
 - if** condition (a) (b) (d) are satisfied **then**
 - delete p ;
 - end if**
 - **end for**

Output: Dendritic skeleton of image I_{ske} .

In this study, the operation for finding branch points is a two-dimensional convolution of the binary image of skeletons and a 3-by-3 filter, with an intensity value of 0 for 4 vertices and 1 for the rest positions. The points with an intensity value equal or greater than 4 are considered as branch points. Figure 8(6) illustrates the branch point detection results.

Locating dendritic spines

We locate the suspected dendritic spines as follows: 1) Remove spur pixels of the dendritic skeletons. The removed pixels are the putative locations of the dendritic spines. 2) In a bifurcation-centered and properly sized region of skeleton, if there is an alternative point connected with the branch point, we consider the alternative point indicates the position of dendritic spine. This process is illustrated in Fig. 10 and the detail is stated in Algorithm 4.



Fig. 10 Illustration of locating dendritic spines. From left to right: Skeleton, skeleton after removing spur pixels, the overlapped image. The red point is the position of dendritic spine (within the red square) and the structure marked by yellow is the overlapped section of the skeleton and skeleton after removing spur pixels

Filtering points on axons

The transgenic mouse used in this study is YFP-H line, in which a subset of layer 5 cortical neurons express YFP. Therefore, YFP signals in these images contain both dendrites and axons. When searching for dendritic spines, it is essential to determine whether these points are on an axon. For each of the structures that centered on suspected spines with a proper size, illustrated in Fig. 11, we take the ratio of its area to its perimeter and average intensity as judging criteria.

As shown in Fig. 12, the positions marked with red circles are the results before screening and the positions marked with green plus sign are results after screening. The positions only marked with red circle are likely locations of axons, rather than spines. The detail is presented in Algorithm 7.

Detection of synapses

Through the discussion in the previous two sections, we obtained the position of the axonal boutons and dendritic spine in the two-photon image stacks. As mentioned in above section, the presynaptic part is located on an axon and the postsynaptic part is located on a dendrite in mostly synapses. Then, it is reasonable to get the locations of the synapses on 2D by integrating the locations of the axon boutons and dendritic spines.

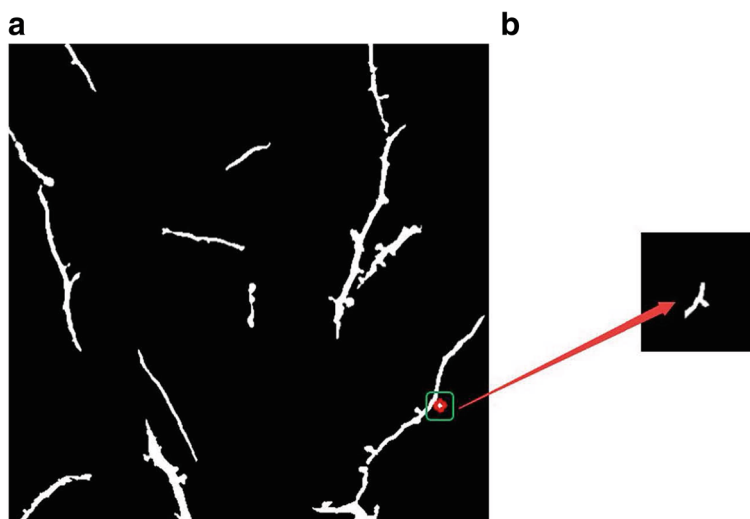


Fig. 11 Illustration of filtering spines on points. **a** binary image of dendrites (left) **(b)** structure centered on suspected spine marked by red circle (right)

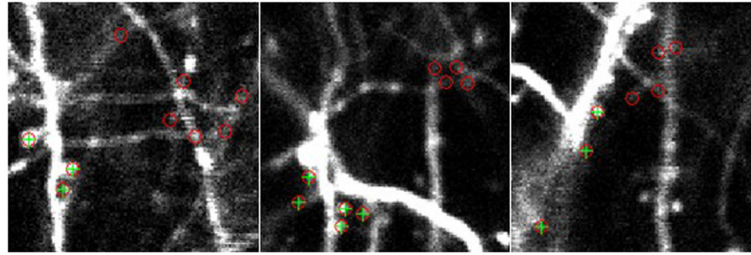


Fig. 12 Comparison of results before and after screening on three different layers

Algorithm 7 Filtering false positives on axons

Input: The coordinates of dendritic spines Ω' .

- **for** each pair of coordinate $ps \in \Omega'$ **do**
 - B_{ps} is part of binary image B obtained by Algorithm 6, which is centered on the spur pixel ps calculated by Algorithm 4;
 - if** the ratio of area to perimeter about white pixels in binary image B_{ps} & average intensity value of normalized image I at the white pixels position in binary image B_{ps} are greater than predefined thresholds respectively **then**
 - Add ps into Ω (predefined by Algorithm 4);
 - end if**
- **end for**

Output: Set of coordinates of filtrated dendritic spines Ω .

Specifically, we calculate the distance between the axon and dendritic spine to determine whether the two are overlapping. Furthermore, we can count the synapses on 3D based on the detection in continuous 2D images. As shown in Algorithm 8, for each synapse in the 2D image, find its nearest synapse in the next layer. If this synapse is also the nearest of the synapse in the next layer, and the distance between them is close enough, these two synapses are the same synapse in the view of 3D.

Algorithm 8 Object counting in 3D

Input: Continuous image stacks $\{S\}$ and threshold t_s

Initialize: $N = 0$

for section $S_i \in \{S\}$ **do**

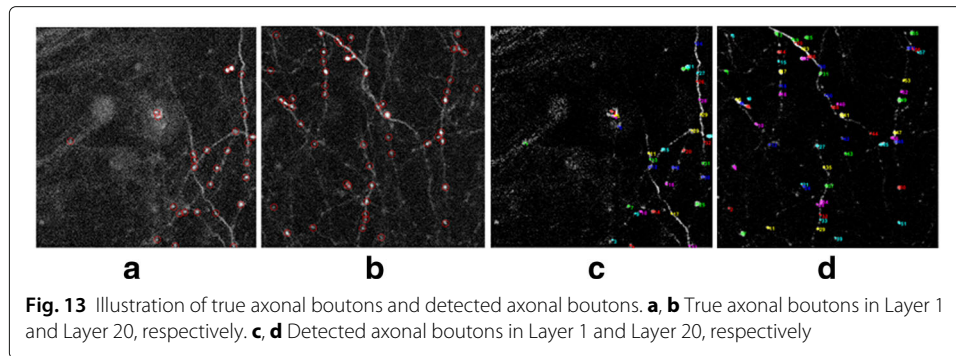
for object $c_j^{(i)}$ on S_i **do**

- Find the closest object in section S_{i+1} , represented the object and the distance as $c_k^{(i+1)}$, $\mathcal{D}_{j,k}^i$ respectively;
- **if** c_j^i is not the closest object to $c_k^{(i+1)}$ in section S_i in turn or $\mathcal{D}_{j,k}^i > t_s$ **then**
 - $N = N + 1$;
- **end if**

end for

end for

Output: Number of the objects in 3D: N .



Experimental results

In order to demonstrate the effectiveness of the proposed algorithm, we show two axon images corresponding to layer 1 and layer 20, with the axonal boutons indicated by red circles marked by experienced neurobiologists in Fig. 13a and b. The corresponding experimental results detected by our algorithm are shown in Fig. 13c and d. The ground truth of synapses, axons and dendrites were redundantly marked by three students, and disagreements are decided by another biologist.

The manual annotation process lasts about 2 days. The round-like structures and the structures shown in Fig. 7 were labeled as axonal boutons and dendritic spines respectively, while the spine-bouton pairs were marked as synapses.

We conducted some experiments on other layers and recorded the number of axonal boutons in ground truth. By comparing the detected result with the corresponding ground truth, we respectively determined the number of redundant and missing axonal boutons in different layers as listed in Table 1.

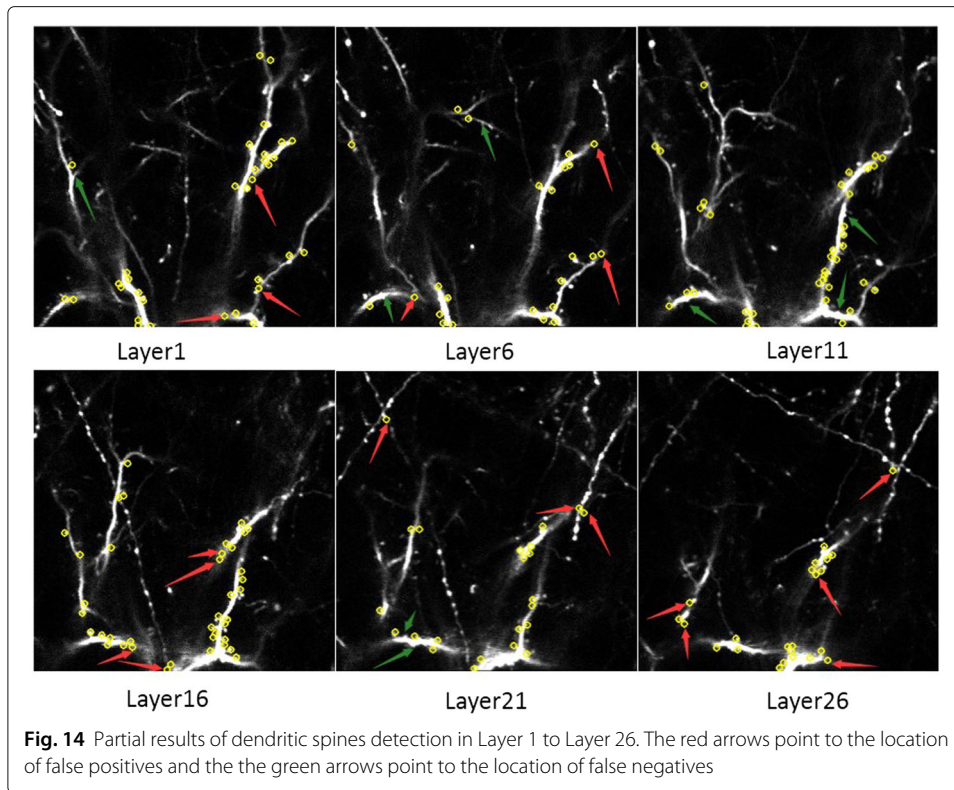
To illustrate the effectiveness of the proposed algorithm, we show partial results of the dendritic spines detection from Layer 1 to Layer 25 in Fig. 14.

As shown in Table 2, we recorded the number of dendritic spines in ground truth and the number of false positive and missing dendritic spines, which were obtained by comparing the detected result with the corresponding ground truth, for several layers.

In Fig. 15, we can see that one axonal bouton indicated by green rectangles arises in layers 5-10 but is only marked in layer 5. Analogously, two axonal boutons are respectively indicated by red rectangles and yellow rectangles are solely marked in layer 8. This method can count the axonal boutons precisely in 3D because it considers the multi-layer information. A specific example in Fig. 16 can account for it.

Table 1 The numerical analysis of experimental result on detected axonal boutons in each layer

Image	Manual	Our method		
		Total	False positive	False negative
layer 1	29	33	4	0
layer 20	50	54	6	2
layer 40	58	62	5	1
layer 60	90	94	7	3
layer 80	86	89	5	2
layer 100	57	62	5	0
Average (/perception)	61.7	65.8	5.3	1.3

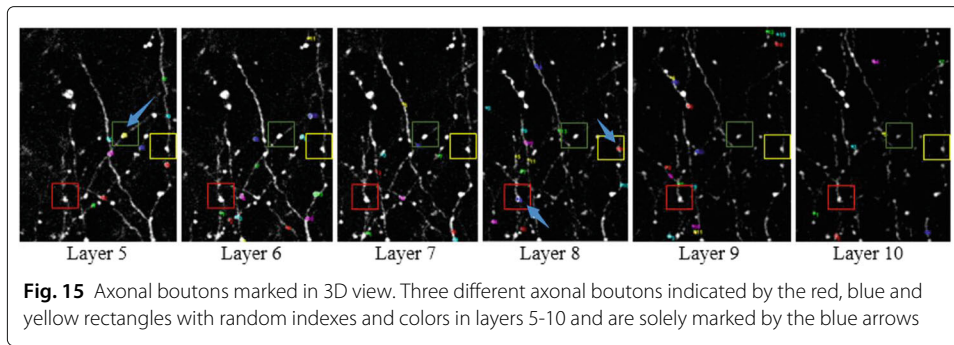


The partial results of synapse detection from Layer 1 to Layer 26 are shown in Fig. 17 and the experimental results of synapse detection are shown in Table 3. The green ellipses mark the location of false negatives and the red arrows point to the location of false positives.

We have integrated the proposed method of identifying axonal boutons, dendritic spines and synapses with TrakEM, a plugin of ImageJ. This automates synapse analysis process. The left subgraph in Fig. 18 shows the 2D synapse positions, in which synapses are marked by yellow circles. It also provides interactive function, which makes it easy to proofread the detection results. Furthermore, we marked the positions located by the automatic method and by manual annotation with blue triangles and a yellow triangle respectively. The right subgraph of Fig. 18, which was extracted from the left subgraph, and shows the manually marked position (marked by a yellow triangle) with a value of -1.

Table 2 Results of detection dendritic spines on several layers

Image	Manual	Our method		
		Total	False positive	False negative
layer 1	31	33	3	1
layer 6	23	24	3	2
layer 11	40	37	0	3
layer 16	35	39	7	0
layer 21	22	23	5	0
layer 26	18	23	5	0
Average (/perception)	34	29.8	3	0.8



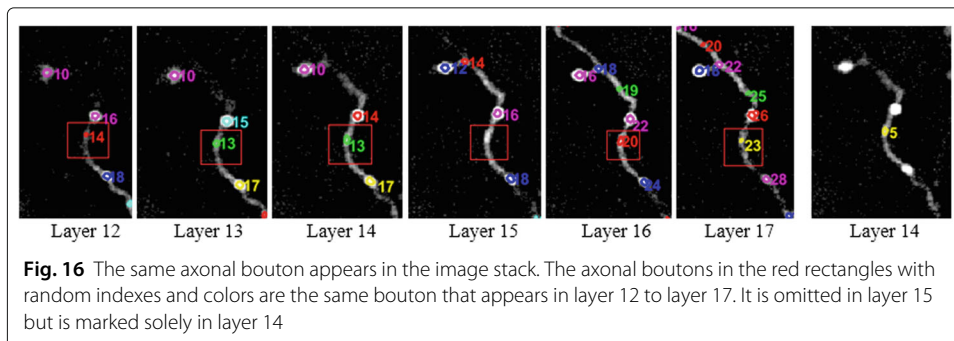
Discussion

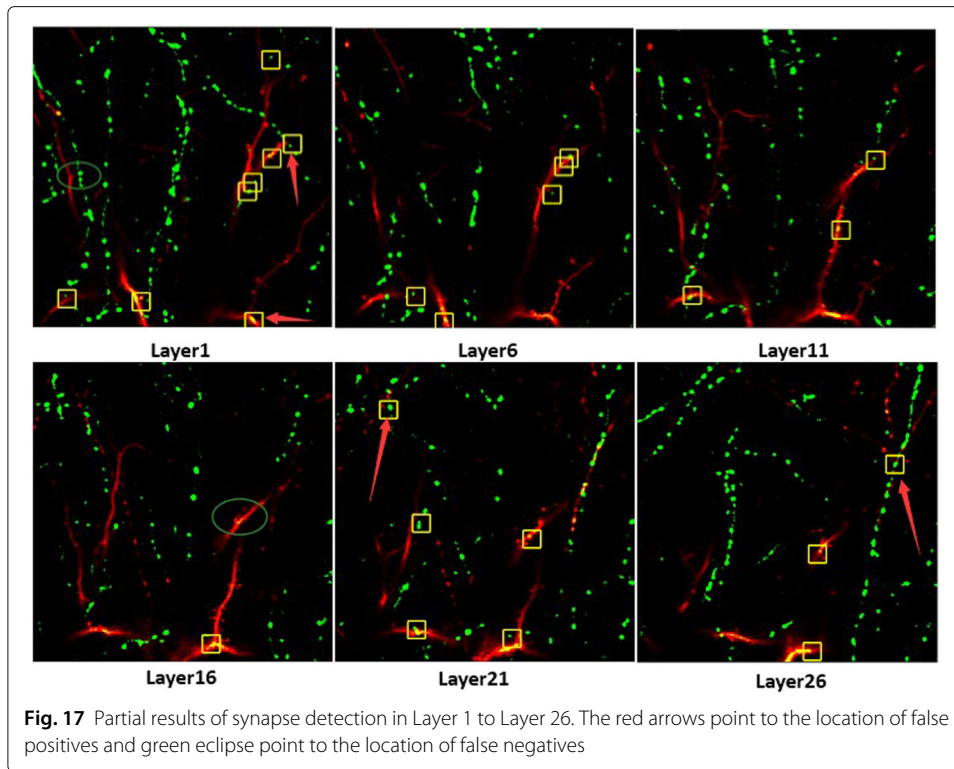
In vivo two-photon microscopy has been widely used to study structural plasticity of axonal boutons and dendritic spines in live animals. Recently, Yang et al. [19] simultaneously labeled and imaged long-range projecting axons and local dendrites, and studied the turnover dynamics of boutons, spines, and synaptic contacts. This dual-color two-photon imaging method allows in vivo examination of synaptic dynamics in specific neural pathways. However, manual annotation of synaptic contacts is time-consuming and prone to bias. The efficiency of synapse detection will be greatly improved by replacing the manual method with automatic method. The automated method can also be used for bouton and spine detection.

As can be seen from the original image in Fig. 1, the structures of axons and dendrites are not significant enough to cause them to be confused with the ambient noise. Therefore, it is necessary to carry out image enhancement to improve the accuracy of detection.

There are 140 two-photon images in total, each of which is 512-by-512 in size with a *x-y-z* resolution of $137 \times 137 \times 700$ nm/pixel. The time spent on manually checking the results of the automatic algorithm and manual annotation are shown in the following bar graph in Fig. 19. We can notice that our approach is much more efficient than manual annotation, especially advantageous if the data volume is larger.

Besides, we have tested our method to another data provided by Beijing Normal University (referred to as Data B) and obtained satisfactory detection results. This dataset provides two-photon image data from neurons in the tbasal ganglia of *aeniopygia guttata*. The volume of the dataset is $53.3 \mu m \times 53.3 \mu m \times 5.6 \mu m$ and slice thickness is $0.2 \mu m$. The size of per image in 2D is $1024 \text{ pixels} \times 1024 \text{ pixels}$. Some of the detection results are shown in Fig. 20, in which the green part are axons and the red part are dendrites. The





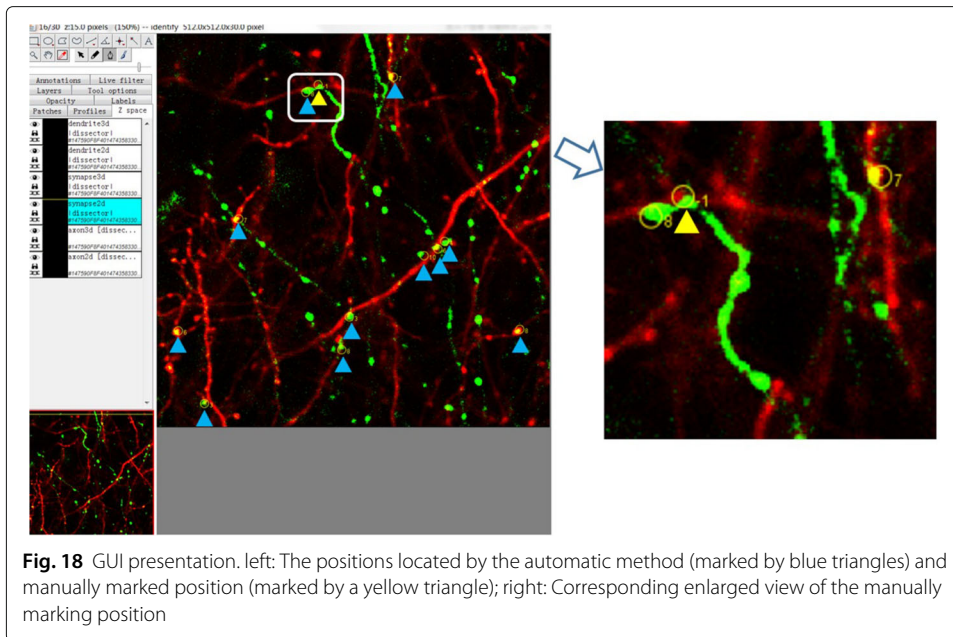
positions of the candidate synapses detected using our pipeline are denoted by blue circles, while the probable missing synapses are indicated by yellow arrows. We detected all 12 synapses in 3D precisely.

Applying our method to a new dataset requires determining the parameters of image enhancement, ie. the radius of axonal bouton and the radius of lines structure of dendrites.

In [29], Yi Zuo et al. found that, using in vivo two-photon imaging, experienced-dependent elimination of postsynaptic dendritic spines in the cortex was accelerated in ephrin-A2 knockout mice and ephrin-A2 regulates experience-dependent, N-methyl-Daspartate (NMDA) receptor-mediated synaptic pruning through glial glutamate transport during maturation of the mouse cortex. In [30], Ajmal Zemmar et al. tested the effects of Nogo-A neutralization on synaptic plasticity in the motor cortex and on motor learning in the uninjured mature Central nervous system (CNS). According to a series

Table 3 Results of detection synapse on several layers

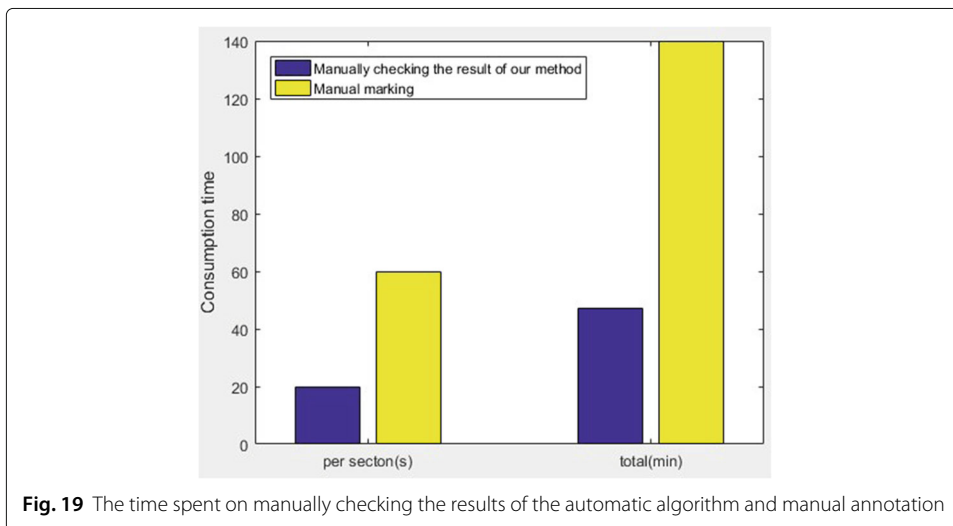
Image	Manual	Our method		
		Total	False positive	False negative
layer 1	8	2	3	1
layer 6	5	0	3	0
layer 11	2	0	0	0
layer 16	1	0	7	1
layer 21	5	0	5	1
layer 26	3	1	5	0
Average (/perception)	2.7	2.8	0.4	0.3

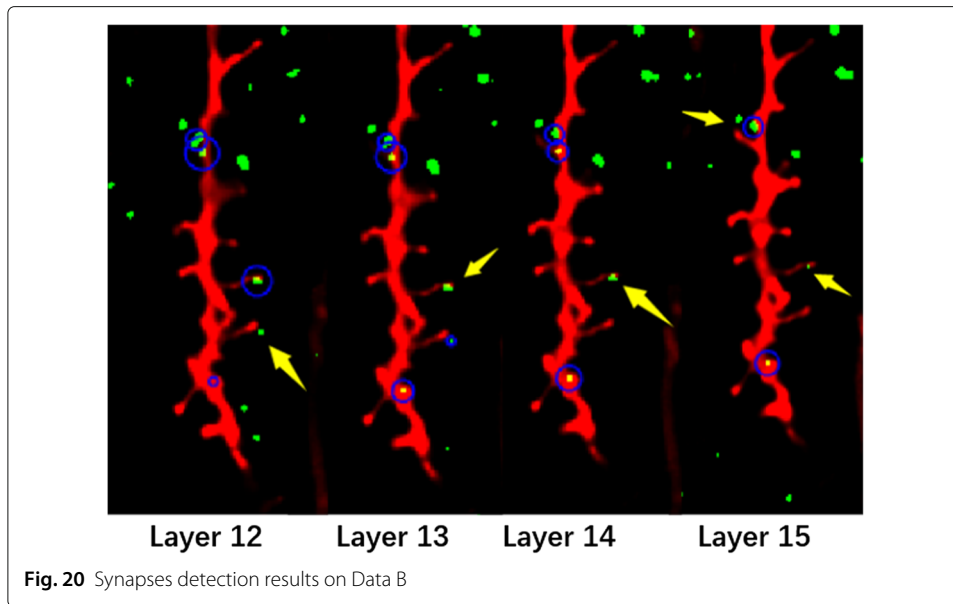


of statistics, such as numbers of dendrites, spines and axons, they concluded that anti-Nogo-A-mediated enhancement of structural and functional synaptic plasticity enlarges the memory capacity per synapse, leading to improved motor learning in vivo. Data analysis in these studies can benefit from our proposed method. Our approach will greatly facilitate data analysis related to dendrite, axon and synapse imaging.

Conclusion

We presented a novel strategy for identifying axon boutons, dendritic spines, and synapses in in vivo two-photon images. For continuous sequence image stack, we can also count the amount of them in 3D by analyzing the context cues of the detected synapses. This approach will help neuroscientists automatically analyze and quantify the formation, elimination and destabilization of the axonal boutons, dendritic spines and synapses. But





it is not yet possible to extract the morphology of synapses. One of our future directions is to get synaptic shapes in 3D.

Appendix 3D deconvolution

The 3D deconvolution operation implemented in ImageJ [22] consists of the following steps:

1. Download the software ImageJ. Then download the following files: Diffraction_PSF_3D.class, Diffraction_PSF_3D.java, Iterative_Deconvolve_3D.class, and Iterative_Deconvolve_3D.java. Next, put files in the plugins folder;
2. Run ImageJ and load the original axon image stacks;
3. Open the Diffraction PSF 3D plugin. Fill the form with the related parameters and compute the point-spread function (PSF);
4. Open the Iterative Deconvolve 3D plugin. Select the generated PSF and original axon image stacks, then input the iteration times and generate the deconvolved axon image stacks.

Appendix A

Model the intensity of axonal bouton using a three-dimensional Gaussian surface:

$$R(x, y) = C \exp\left(-\frac{(x-x_0)^2 + (y-y_0)^2}{2\delta^2}\right).$$

The partial derivatives R_{xx} , R_{xy} , R_{yx} , R_{yy} can be computed as follows:

$$\begin{aligned} R_{xx}(x, y) &= R(x, y) \left(\frac{(x-x_0)^2}{\delta^4} - \frac{1}{\delta^2} \right) \\ R_{xy}(x, y) &= R_{yx}(x, y) = R(x, y) \frac{(x-x_0)(y-y_0)}{\delta^4} \\ R_{yy}(x, y) &= R(x, y) \left(\frac{(y-y_0)^2}{\delta^4} - \frac{1}{\delta^2} \right). \end{aligned} \quad (6)$$

Then the eigenvalues $\lambda_a(x, y)$ of the Hessian matrix are solved as follows:

$$\lambda_a(x, y) = R(x, y) \left(\left((x - x_0)^2 + (y - y_0)^2 - 2\delta^2 \right) \pm \sqrt{\left((x - x_0)^2 + (y - y_0)^2 + 2\delta^2 \right)^2 - 4\delta^4} \right) / 2\delta^4, \quad (7)$$

Appendix B

For clarity of presentation, we choose the cross section of $y = y_0$. The Gaussian curve corresponding to the pixel value of cross section $y = y_0$ is

$$R(x) = C \exp \left(-\frac{(x - x_0)^2}{2\delta^2} \right). \quad (8)$$

And the edge point (x^*, y_0) satisfies

$$(x^* - x_0)^2 + (y_0 - y_0)^2 = r^2 \quad (9)$$

Additionally by the definition in [23], the edge point (x^*, y_0) in (8) also satisfies the equation $R'''(x^*, y_0) = 0$. After some lengthy calculations, we have

$$R(x^*) \left((x^* - x_0)^3 - 3\delta^2 (x^* - x_0) \right) = 0. \quad (10)$$

A suitable solution is

$$x^* = x_0 + \sqrt{3}\delta. \quad (11)$$

According to Eqs. (9) and (11), we conclude that $\delta = r/\sqrt{3}$ is a good choice to identify the axonal boutons.

Appendix C

According to [23], the magnitude of the second derivative of the extracted position is always maximum at the line position. Then, for a fixed $y = y_0$, the third derivative of Formula(4)

$$I(x') = C_{den} \exp \left(-\frac{x'^2}{2\sigma^2} \right) = C_{den} \exp \left(-\frac{(x \cos \theta - y \sin \theta)^2}{2\sigma^2} \right)$$

can be written as:

$$-\frac{I(x \cos \theta - y_0 \sin \theta)}{\sigma^4} (x_0 \cos \theta - y_0 \sin \theta) \left[(x_0 \cos \theta - y_0 \sin \theta)^2 - 3\sigma^2 \right] = 0.$$

Then we can obtain

$$x_0 \cos \theta - y_0 \sin \theta = \sqrt{3}\sigma.$$

With additional efforts, as illustrated in Fig. 9(a), we can obtain the relationship between the variance σ and the radius of the linear structure w :

$$\sigma = w/\sqrt{3}.$$

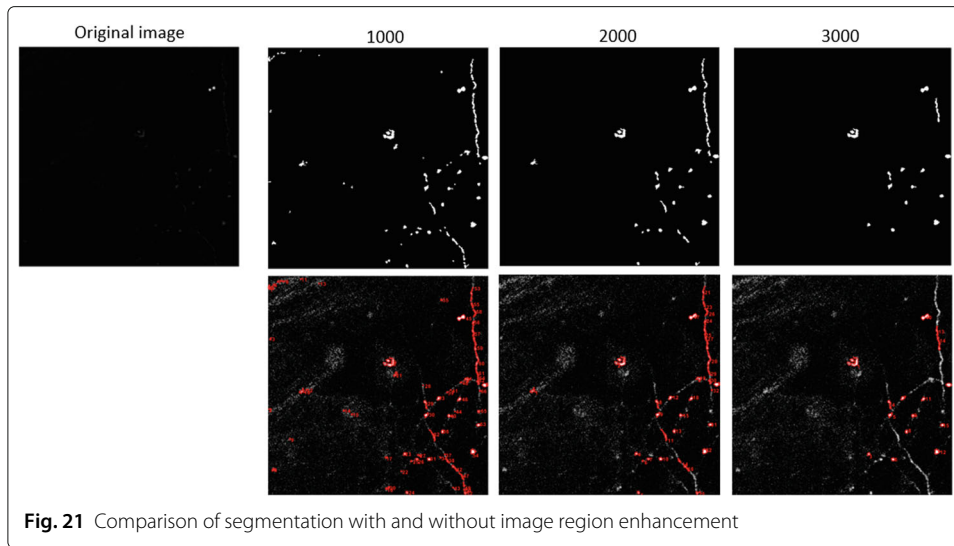


Fig. 21 Comparison of segmentation with and without image region enhancement

Appendix D

For I as shown in Formula(4), the partial derivatives I_{xx} , I_{xy} , I_{yx} , and I_{yy} can be computed as follows:

$$\begin{aligned}
 I_{xx}(x, y) &= I(x, y) \left[\frac{\cos^2 \theta}{\sigma^4} (x \cos \theta - y \sin \theta)^2 - \frac{\cos^2 \theta}{\sigma^2} \right] \\
 I_{yy}(x, y) &= I(x, y) \left[\frac{\sin^2 \theta}{\sigma^4} (x \cos \theta - y \sin \theta)^2 - \frac{\sin^2 \theta}{\sigma^2} \right]
 \end{aligned}
 \tag{12}$$

$$I_{xy}(x, y) = I_{yx}(x, y) = I(x, y) \left[\frac{\sin \theta \cos \theta}{\sigma^2} + \frac{\sin \theta \cos \theta}{\sigma^4} (x \cos \theta - y \sin \theta)^2 \right].
 \tag{13}$$

Then we can get the eigenvalues of $H(x, y) = \begin{pmatrix} I_{xx}(x, y) & I_{xy}(x, y) \\ I_{yx}(x, y) & I_{yy}(x, y) \end{pmatrix}$:

$$\lambda_d(x, y) = -\frac{1}{\sigma^2} \exp \left(-\frac{(x \cos \theta - y \sin \theta)^2}{2\sigma^2} \right)
 \tag{14}$$

Appendix E. Comparison of segmentation with and without image region enhancement

To justify the use of the image region enhancement on boutons, some useful experiments are conducted. We use three different thresholds, 1000, 2000, 3000, for direct segmentation. Above figures provide direct segmentation results without image region enhancement on boutons. Below figures reserve the final segmentation regions containing local maximum value. From these figures, we conclude that a small threshold will

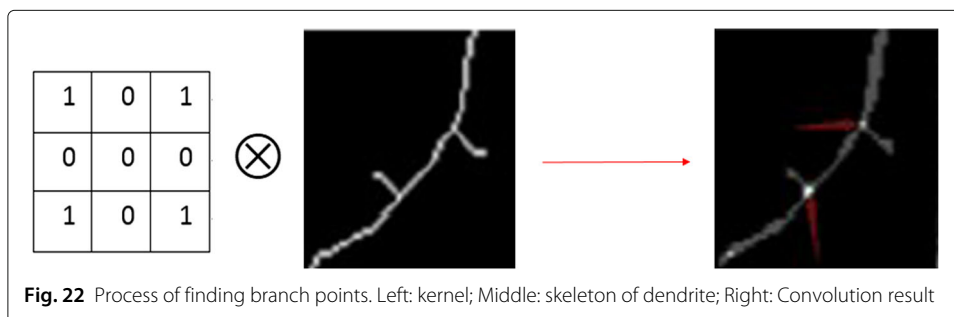


Fig. 22 Process of finding branch points. Left: kernel; Middle: skeleton of dendrite; Right: Convolution result

reserve the bright axon shaft, whereas a big threshold will eliminate the weak axonal boutons. For these reasons, we propose to use the image region enhancement method to extract the disk-like structure. The original experiment results demonstrated the effectiveness of our proposed method.

Appendix F. Process of finding branch points

We show the process of finding branch points in the following figure. The kernel is a 3-by-3 filter with an intensity value of 0 for 4 vertices and 1 for the rest positions. And the points on the convolution result, with an intensity value equal or greater than 4 are considered as branch points.

Abbreviations

CNS: Central nervous system; DAMAS: Deconvolution approach for the mapping of acoustic sources; GFP: Green fluorescent protein; NMDA: N-methyl-D-aspartate; PSF: Point-spread function; YFP: Yellow fluorescent protein

Acknowledgements

Not applicable.

Funding

The financial support of Special Program of Beijing Municipal Science & Technology Commission (NO. Z16110000216146), Science and Technology Development Fund of Macau (044/2015/A2), Scientific research instrument and equipment development project of Chinese Academy of Sciences (YZ201671), Strategic Priority Research Program of the CAS (NO. XDB02060001), Institute of Automation, CAS, for the 3D Reconstruction of Brain Tissue at Synaptic Level (NO. Y3J2031DZ1) and National Natural Science Foundation of China (NO. 61673381, NO. 61201050, NO. 61306070, No. 31472001) is appreciated.

Availability of data and materials

The data and source code in this paper is available upon request.

Authors' contributions

Conceived and designed the experiments: QX, XC, HH, YY Performed the experiments: QX, HD Analyzed the data: QX Contributed materials: DL, YY, YS, XZ. All authors read and approved the final manuscript.

Ethics approval and consent to participate

Not applicable.

Consent for publication

Not applicable.

Competing interests

The authors declare that they have no competing interests.

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Author details

¹Research Base of Beijing Modern Manufacturing Development, No.100, Pingleyuan, 100124 Beijing, China. ²Data Mining Lab, School of Management, Beijing University of Technology, No.100, Pingleyuan, 100124 Beijing, China. ³Institute of Automation, Chinese Academy of Sciences, 95 Zhongguancun East Road, 100190 Beijing, China. ⁴Faculty of Information Technology, Macau University of Science and Technology, Avenida Wai Long, Taipa, Macau, China. ⁵Institute of Neuroscience, Chinese Academy of Sciences, 320 Yue Yang Road, 200031 Shanghai, China. ⁶Beijing Normal University, No. 19, Waida Jie, Xijie Kou, 100875 Beijing, China. ⁷Center for Excellence in Brain Science and Intelligence Technology Shanghai Institutes for Biological Sciences, Chinese Academy of Sciences, 320 Yue Yang Road, 200031 Shanghai, China. ⁸University of Chinese Academy of Sciences, School of future technology, No.19(A) Yuquan Road, 100049 Beijing, China.

Received: 16 April 2017 Accepted: 4 December 2017

Published online: 20 December 2017

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